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Перспективы применения компьютерного зрения для выявления камней в мочевыделительной системе и новообразований печени и почек на изображениях компьютерной томографии органов брюшной полости и забрюшинного пространства



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АННОТАЦИЯ

В работе представлен селективный обзор литературы, посвящённый использованию алгоритмов компьютерного зрения для диагностики новообразований печени и почек, а также камней в мочевыделительной системе на изображениях компьютерной томографии органов брюшной полости и забрюшинного пространства.

В обзор были включены статьи, опубликованные за период с 01.01.2020 по 24.04.2023 гг.

В задаче сегментации печени и её новообразований алгоритмы, оперирующие пикселями, показали наибольшие значения параметров диагностической точности (точность достигает 99,6%; коэффициент сходства Дайса — 0,99). Задачи классификации новообразований печени на текущий момент лучше решаются воксельными алгоритмами (точность до 82,5%).

Сегментация почек и их новообразований, а также классификация опухолей почек одинаково хорошо выполняются алгоритмами, анализирующими как пиксели, так и воксели (точность достигает 99,3%, коэффициент сходства Дайса — 0,97).

Алгоритмы компьютерного зрения в настоящее время также способны с высокой степенью точности определять конкременты в мочевыделительной системе размерами от 3 мм (точность достигает 93,0%).

Таким образом, существующие алгоритмы компьютерного зрения позволяют не только эффективно выявлять новообразования печени и почек, а также конкременты в мочевыделительной системе, но и с высокой точностью определять их количественные и качественные характеристики.

Более высокая точность определения вида новообразования может быть достигнута за счёт оценки воксельных данных, поскольку в этом случае алгоритм анализирует новообразование полностью в трёх измерениях, а не только в плоскости одного среза.

Ключевые слова: компьютерная томография; нейронные сети; глубокое машинное обучение; органы брюшной полости; мочекаменная болезнь; образования почек; образования печени.

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REVIEWS

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Prospects of using computer vision technology to detect urinary stones and liver and kidney neoplasms on computed tomography images of the abdomen and retroperitoneal space

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ABSTRACT

The article presents a selective literature review on the use of computer vision algorithms for the diagnosis of liver and kidney neoplasms and urinary stones using computed tomography images of the abdomen and retroperitoneal space. The review included articles published between January 1, 2020, and April 24, 2023. Pixel-based algorithms showed the greatest diagnostic accuracy parameters for segmenting the liver and its neoplasms (accuracy, 99.6%; Dice similarity coefficient, 0.99). Voxel-based algorithms were superior at classifying liver neoplasms (accuracy, 82.5%). Pixel- and voxel-based algorithms fared equally well in segmenting kidneys and their neoplasms, as well as classifying kidney tumors (accuracy, 99.3%; Dice similarity coefficient, 0.97). Computer vision algorithms can detect urinary stones measuring 3 mm or larger with a high degree of accuracy of up to 93.0%. Thus, existing computer vision algorithms not only effectively detect liver and kidney neoplasms and urinary stones but also accurately determine their quantitative and qualitative characteristics. Evaluating voxel data improves the accuracy of neoplasm type determination since the algorithm analyzes the neoplasm in three dimensions rather than only the plane of one slice.

Keywords: computed tomography; neural networks; deep learning; abdomen; urolithiasis; renal neoplasms; liver neoplasms.

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计算机视觉在腹部和腹膜后计算机断层扫描图片上检 测泌尿系统结石和肝肾肿块的应用前景

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摘要

本文对计算机视觉算法在腹部和腹膜后计算机断层扫描图片被用于诊断肝肾肿块以及泌尿系统结石的情况进行了有选择性的文献综述。

综述中的文章发表于2020年1月1日至2023年4月24日。

在肝脏及其肿块的分割任务中,使用像素算法显示出最高的诊断准确率参数值(准确率达到 99.6%; Dice相似系数为0.99)。目前,基于体素的算法能较好地解决肝肿块分类任务(准确率高达82.5%)。

通过分析像素和体素的算法,肾脏及其肿块的分割和肾肿块的分类同样出色(准确率达到 99.3%,Dice相似系数为0.97)。

现在,计算机视觉算法也能高度准确地检测出泌尿系统中3毫米及以上大小的结石(准确率达到93.0%)。

因此,现有的计算机视觉算法不仅能有效检测肝肾肿块以及泌尿系统中的结石,还能高度准 确地确定它们的定量和定性特征。

通过评估体素数据,可以提高肿块类检测的准确度。在这种情况下,算法会对整个肿块进行 三维分析,而不仅只是在一个切片的平面上进行分析。

关键词: 电子计算机断层扫描; 神经网络; 深度机器学习; 腹部器官; 泌尿系结石病; 肾肿 块; 肝肿块。

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INTRODUCTION

X-ray diagnosis has greatly evolved in recent years. In particular, computer vision technology has been actively employed for the interpretation of computed tomography (CT) scans for more accurate and timely diagnosis and reduction of the burden on medical personnel [1–3]. Several artificial intelligence algorithms for the analysis of chest CT scans have already demonstrated high accuracy in specific disease areas (with the area under the receiver operating characteristic curve reaching 0.88) [3].

Moreover, computer vision technology is extensively used in the diagnosis of abdominal pathologies. In the last 5 years, the number of PubMed publications on this topic has increased 12 times, i.e., from 34 in 2018 to 411 in 2022. The dramatic increase in the number of studies could be attributed to increased CT availability to the general population, a relatively broad and growing list of diagnosed disorders, and the high accuracy of their verification using CT scans.

Currently, ready-made computer vision-based solutions are capable of detecting common pathologies such as liver and kidney neoplasms and urinary stones using abdominal and retroperitoneal CT scans [4].

These solutions are based on algorithms that can be classified into two types based on their function:

- 1. Algorithms identifying (segmenting) organs and their pathologies
- 2. Algorithms classifying the pathology

The described solutions offer variable levels of diagnostic accuracy, which could be attributed to the architecture of deep-learning networks and computer vision algorithms. Deep machine-learning architectures based on convolutional neural networks are currently most commonly used for classification [5].

This review aimed to assess the diagnostic accuracy and architecture of computer vision algorithms for detecting liver and kidney neoplasms and urinary stones on CT scans, depending on the algorithm function (segmentation or classification).

SEARCH METHODOLOGY

An analytical study was performed: it was a selective literature review of algorithms intended for primary diagnosis of common conditions such as liver and kidney neoplasms and urinary stone disease.

Other common neoplasms, such as pancreatic tumors, can be detected on abdominal and retroperitoneal CT. However, this review focused on liver and kidney neoplasms and urinary stones. If any, few studies have used computer vision technology to detect neoplasms of other organs in these anatomical areas.

The literature search was performed in PubMed (accessed on April 30, 2023) using the following keyword combinations:

["Deep Learning," "Neural Network," "Artificial Intelligence"] + ["Liver Tumor," "Kidney Tumor," "Hepatocellular Carcinoma," "Kidney Stone"] + "Computed Tomography".

A search was also performed in eLibrary, the Russian electronic research library and information analysis system for science citation index (accessed on April 30, 2023), from 2019 to the present using the keywords "Artificial intelligence" + "Computed Tomography". However, the search failed to identify publications on deep-learning algorithms for detecting abdominal and retroperitoneal organ disorders.

The analysis included studies identified in PubMed that used computer vision algorithms for segmentation and classification of pathologies of interest on abdominal and retroperitoneal CT scans, described the deep-learning algorithm architecture, and presented the results of the algorithm performance using one of the following parameters: Dice coefficient for segmentation and accuracy and F1-score or area under the ROC curve (AUC) for classification [6].

The search covered the period from January 1, 2020, to April 24, 2023.

RESULTS

The review included 21 studies, and their findings are presented in Appendix 1. The architecture was analyzed, and diagnostic metrics were assessed in the selected studies. Moreover, these studies were compared with other publicly available articles not included in the analysis.

Liver neoplasms

Contrast-enhanced CT and magnetic resonance imaging (MRI) are currently the most informative methods for the diagnosis of liver neoplasms [7]. CT offers various advantages over MRI, such as equipment availability, expert qualification, testing time, and cost-effectiveness [8]. Contrast enhancement is a common strategy when a liver neoplasm is suspected because non-contrasted scans are less informative. However, in some other diseases, noncontrasted abdominal CT is often performed. The ability of computer vision algorithms to detect liver neoplasms on non-contrasted CT scans may be used for screening for this pathology [9–11].

The U-Net architecture and its modifications (i.e., ResNet blocks) are most widely used for segmentation of the liver and liver neoplasms, with acceptable diagnostic accuracy. H. Rahman et al. demonstrated the best results for the segmentation of the liver and liver neoplasms using ResUNet, with a Dice coefficient of 0.09 and an accuracy of 99.6% [12]. An example of liver neoplasm segmentation is presented in Fig. 1.

Pixel-based (2D image) segmentation algorithms had better diagnostic metrics than voxel-based (3D image) segmentation algorithms [12–18].

In turn, voxel-based algorithms show better diagnostic metrics in liver neoplasm classification. These algorithms

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Fig. 1. An example of liver neoplasm segmentation using one of the algorithms.

demonstrate high reliability in distinguishing benign tumors from malignancies (accuracy up to 85.5%). The accuracy of determining a specific type of malignant neoplasms is currently lower at only 73.4% [19, 20].

Despite the development and widespread use of deep machine-learning, some classic machine-learning algorithms (e.g., support vector machine [SVM]) also demonstrate high diagnostic metrics in liver neoplasm classification, with an accuracy of up to 84.6% [19, 21].

The Center for Diagnostics and Telemedicine (Moscow) is currently developing a computer vision algorithm using contrast enhancement for within-class segmentation and differentiation of liver masses. An example is presented in Fig. 2.

Kidney neoplasms

In 27%-50% of cases, kidney neoplasms are asymptomatic and represent random findings [22]. CT allows



Fig. 2. An example of liver neoplasm segmentation by an algorithm based on a contrast-enhanced CT scan.

for the assessment of the tumor location and size and the relationship between the tumor and renal pelvis and large vessels.

In the analyzed studies, the U-Net architecture and its modifications are most widely employed for the segmentation of the kidneys and kidney neoplasms. The Dice coefficient for kidney segmentation currently reaches 0.97 with the U-Net 3D architecture [23]. The same architecture provided the highest Dice coefficient for kidney tumor and kidney cyst segmentation (0.84 and 0.54, respectively). Thus, the accuracy of kidney neoplasm segmentation is currently inferior to that of kidney segmentation. Moreover, voxel-based architectures demonstrated diagnostic accuracy metrics for the segmentation of the kidneys and kidney neoplasms on CT scans noninferior to those of classic pixel-based algorithms [23–26].

Other architectures (e.g., EffectiveNet) also demonstrate a high Dice coefficient for the segmentation of the kidneys and kidney neoplasms (up to 0.95) [27, 28]. An example of kidney neoplasm segmentation is presented in Fig. 3.

Both classic machine-learning algorithms and deeplearning algorithms are used for the classification of kidney neoplasms [24, 26, 29–31]. Swin transformers architectures have the greatest accuracy (99.3%) [29].

When data are limited, classic machine-learning algorithms and feedforward architectures prove effective [26]. Similarly to the segmentation of the kidneys and kidney neoplasms, the classification performance of voxel-based architectures is noninferior to that of pixelbased architectures [31].

Urinary stone disease

Urinary stone disease is the second most commonly detected urological condition [32]. The incidence and

prevalence of urinary stone disease in adults are steadily increasing throughout the Russian Federation. According to N. Gadzhiev et al., the prevalence of urinary stone disease has increased by 35.4% in 15 years, whereas the incidence has reached 16.2% [33].

Retroperitoneal CT is the gold standard for the diagnosis of urinary stone diseases. It allows for the assessment of the location, size, and number of radiopaque urinary stones with sensitivity and specificity of up to 96% and 100%, respectively [34].

The articles showed a direct association between the accuracy of urinary stone detection and the size of urinary stones. The accuracy of convolutional neural network-based algorithms increases with the size of urinary stones [35, 36]. To illustrate, the accuracy rates of detecting urinary stones <1, 1-2, and >2 cm were 85%, 89%, and 93%, respectively.

The Swin transformers algorithm has currently the greatest accuracy in urinary stone detection (98%) [29]. An example of urinary stone detection using one of the algorithms is presented in Fig. 4.

The use of computer vision algorithms for the diagnosis of urinary stone diseases can be challenging if small atherosclerotic plaques are present in renal artery walls because their densities are similar to those of urinary stones [36].

Modern deep machine-learning and computer vision technologies allow for the detection of urinary stones measuring ≥ 3 mm with low radiation exposure, and urinary stones measuring ≥ 5 mm are considered clinically significant [37].

Determining the urinary stone type is one of the most important factors for the future treatment strategy [35, 37]. Numerous CT-based parameters have been employed



Fig. 3. An example of right kidney neoplasm segmentation.



Fig. 4. An example of urinary stone detection using one of the algorithms.

in assessing postoperative prognosis (such as relapsefree disease) and determining the urinary stone type using machine-learning technology [38–41]. Several studies of dual-energy CT confirm that this imaging technique can also be used for assessing the chemical composition of urinary stones [42, 43]. However, this method has several limitations, most notably, its low applicability in routine clinical practice [44].

According to Y. Cui et al., narrowly specialized convolutional neural networks allow for the assessment of urinary stones using the STONE nephrolithometry score, and results were comparable to radiologist opinions [45]. This approach also allows for the assessment of prognossis [46].

DISCUSSION

Several studies have used publicly available datasets, such as LiTS, KiTS'19, and 3D-IRCADb, and most of them include contrast-enhanced CT findings. The datasets of studies using their CT scans mostly included contrastenhanced CT findings or mixed data.

The analysis revealed that modern deep-learning algorithms provide high accuracy liver segmentation (maximum Dice coefficient, 0.99; mean Dice coefficient, 0.92 \pm 0.09) and kidney segmentation (maximum Dice coefficient, 0.97; mean Dice coefficient, 0.94 \pm 0.02) on CT scans (Appendix 1).

Pixel-based algorithms show better diagnostic accuracy metrics for liver segmentation (maximum Dice coefficient, 0.99; mean Dice coefficient, 0.97±0.01), whereas voxel-based algorithms are noninferior to pixel-based algorithms for kidney segmentation. This could be attributed to differences in the size and density of these solid organs and the history of algorithm development. Voxel-based algorithms have higher performance requirements. Such computer-based systems have only recently become widely available. Currently, improved pixel-based algorithms are being developed in research centers.

Liver and kidney neoplasm segmentation is less accurate than liver and kidney segmentation, which is primarily due to incomplete neoplasm segmentation. The correct determination of neoplasm borders depends on their growth type and structure; thus, the best segmentation is observed for exophytic heterogeneous neoplasms [23]. This is also why isodense cysts and hemangiomas are segmented with low accuracy [20].

Data preprocessing before using a segmentation algorithm resolves this issue to some extent [27, 28]. K. Yildirim et al. found that analyzing alternative CT slices, such as sagittal or coronal, using deep machine-learning algorithms also contributes to the accuracy of pathology detection [47].

According to the literature review, voxel-based algorithms are more suitable for neoplasm classification than pixel-based algorithms because the structure of the tumor is indicative of its nature [19, 26, 31]. Deep-learning technology provides highly accurate classification of benign and malignant abdominal neoplasms [19, 20, 31].

The completeness of segmentation is critical for the accuracy of subsequent classification. Currently, a combination of two-dimensional algorithms can be used for segmentation and a combination of three-dimensional (3D) algorithms for classification [19, 24]. Moreover, a combination of deep- and classic machine-learning algorithms (including gradient boosting) can improve diagnostic metrics [19]. The studies analyzed used two types of combinations of these algorithms. L. Yang et al. and M. Shehata et al. proposed creating features by algorithmic methods and using them in a feedforward network [30, 31]. Meanwhile, E. Trivizakis et al. and X.L. Zhu et al. proposed creating features using deep-learning networks and classifying them using classic machine-learning algorithms [19, 26].

Equally important is using a transformer architecture for neoplasm classification; however, its application is limited by the availability of training data. Obtaining high metrics when using transformer architectures requires significantly more training data than with high accuracy neural networks [29].

The studies analyzed used conventional quality assessment metrics for deep machine-learning algorithms. However, the research methodology varied among studies, making comparative assessment of diagnostic accuracy difficult. Most authors did not provide the 95% confidence interval for diagnostic accuracy parameters, which was an additional limitation and prevented assessment of the significance of differences between metrics obtained using different neural network architectures and approaches. A standardized assessment can be useful in determining algorithms with the best results [48]. Some of the analyzed studies also had small samples.

Another possible use of deep machine-learning algorithms is to improve the quality of low-dose CT scans. For example, F.R. Schwartz et al. proposed using deep machine-learning algorithms for data interpolation and reconstruction in DECT [49–51]. This approach allows for the acquisition of high-energy CT scans with a low radiation exposure.

Thus, computer vision algorithms have already demonstrated good diagnostic accuracy parameters in detecting urinary stones and liver and kidney neoplasms on CT scans. The next goal is to implement computer vision technology in healthcare facilities for more accurate and timely diagnosis and reduction of the burden on medical personnel. More large-scale, well-designed prospective studies are warranted to assess the efficacy of artificial intelligence-based software in detecting abdominal neoplasms during screening and for their qualitative and quantitative assessment with subsequent verification of the results.

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CONCLUSION

Existing computer vision systems for assessing abdominal and retroperitoneal CT scans effectively detect liver and kidney neoplasms and urinary stones. Moreover, these systems allow for the accurate determination of their quantitative and qualitative parameters. Further technological advancements will improve 3D deep-learning algorithms and their diagnostic accuracy, ensuring more accurate results, particularly for multiclass classification. Voxel data can provide a more accurate determination of the pathology type because, in this case, algorithms ensure the 3D analysis of neoplasms rather than a single-slice analysis.

A more thorough analysis of data obtained using computer vision technology can be used to determine the effectiveness of contrast-enhanced CT scans. Methods for improving CT scan quality will make it possible to take scans only during specific phases (e.g., arterial and excretory phases) depending on the study purposes, reducing the effective radiation dose.

ADDITIONAL INFORMATION

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				itaset) dataset
Segmentation of the liver – Dice coefficient: 0.77 – Accuracy: 93%	 Segmentation of the liver Dice's coefficients: 0.97 for the Dircadb dataset 0.97 for the LiTS dataset 0.95 for the Sliver07 dataset 0.95 for the Chaos dataset 0.95 for the Dircadb dataset 0.97 for the Dircadb dataset 0.97 for the LiTS dataset 0.97 for the LiTS dataset 	Segmentation of the liver and liver neoplasms: – Dice coefficient: 0.99 – Accuracy: 99.6%	Segmentation of the liver Dice coefficients: - 0.86 for the 3D MultiRes U-Net - 0.84 for the 3D Dense U-Net - 0.73 for the 3D U-Net	Segmentation of liver neoplasms Dice coefficients: – 0.96 for the 3D U-Net + LSSC + MA with the LiTS da – 0.96 for the 3D U-Net + LSSC + MA with the Dircadl – 0.92 for the 3D U-Net with the LiTS dataset – 0.89 for the 3D U-Net with the Dircadb dataset
ResUNet with multiscale parallel convolution blocks after Res blocks	ResUNet basic block: three sequential Conv2D layers with kernel-based convolution expansion (three expansion rates: 1, 2, and 4)	Sequential use of ResUNet for liver segmentation, with subsequent use of the findings in another ResUNet for neoplasm segmentation	Three 3D U-Net modifications: 1) 3D U-Net and classic network 2) 3D MultiRes U-Net. The resolution path block is used before skip connection. Inside the Conv block: three linked 3D convolutions, $3\times3\times3$ (first, 32 filters; remainder, 16 filters each), which are pooled, normalized, and summed up with input data processed using Conv3D ($1 \times 1 \times 1$, 64 filters). This is followed by sigmoid activation. 3) 3D Dense U-Net: with residual pooling after each Conv layer	3D MAD-UNet: Long-short skip connection (LSSC) and attention module are used for all decoder levels.
4 studies	3 studies (Dircadb) 19 studies (LiTS) 4 studies (Silver07) 1 study (Chaos)	4 studies	1 study	8 studies (Dircadb) 15 studies (LiTS)
M. Maqsood et al., 2021 [13]	R.Z. Khan et al., 2022 [14]	H. Rahman et al., 2022 [12]	A. Affane et al., 2021 [15]	J. Wang et al., 2023 [17]
		ntation of the liver	structures	
	M. Maqsood et 4 studies ResUNet with multiscale parallel convolution blocks after Res 2021 [13] 4 studies blocks - Dice coefficient: 0.77 – Accuracy: 93%	M. Maqsood et al., 2021 [13] 4 studies blocks ResUNet with multiscale parallel convolution blocks after Res Dice coefficient: 0.77 Segmentation of the liver Dice coefficient: 0.77 M. Maqsood et al., 2021 [13] 4 studies (13] ResUNet with multiscale parallel convolution blocks after Res Dice coefficient: 0.77 Dice coefficient: 0.77 R.Z. Khan et al., 1 study (Chaos) 3 studies (Dircadb) 1, 2, and 4) ResUNet basic block: three sequential Conv2D layers with 0.97 for the Dircadb dataset 0.97 for the Chaos dataset 0.97 for the Chaos dataset 0.97 for the Chaos dataset 0.97 for the Chaos dataset 0.97 for the Dircadb dataset 0.97 for the Chaos dataset 0.97 for the Chaos dataset 0.97 for the Dircadb dataset 0.97 for the Chaos dataset 0.97 for the Dircadb dataset	M. Maqsood et al., 2021 [13] 4 studies blocks ResUNet with multiscale parallel convolution blocks after Res blocks Segmentation of the liver - Dice coefficient: 0.77 - Accuracy: 93% R.2. Khan et al., 1 studies (Dircadb) 3 studies (Dircadb) R.2. Khan et al., 1 studies (SilverOT) 1.5 segmentation of the liver Dice's coefficients: - 0.97 for the Dircadb dataset - 0.97 for the LiTS dataset - 0.97 for the LiTS dataset - 0.97 for the LiTS dataset - 0.97 for the Dircadb dataset - 0.97 for the LiTS dataset - 0.97 for the liver and liver neoplasms	M. Mageood et al., 2021 [13] A studies blocks ResUNet with multiscale parallel convolution blocks after Res Dice's coefficient: 0.77 Segmentation of the liver - Accuracy 93% R.Z. Khan et al., 1 study (Chaos) 3 studies (LTS) (15) ResUNet basic block: three sequential Com/2D layers with 1 study (Chaos) 0.37 for the Diradb dataset 0.37 for the Diradb dataset 0.37 for the Chaos dataset 0.37 for the Chaos dataset 0.37 for the Chaos dataset 0.32 for the Chaos dataset 0.33 for the Chaos dataset 0.33 for the Chaos dataset 0.33 for the Chaos dataset 0.45 for the Chaos dataset 0.33 for the Ch

Table 1. Continued				
-	2	3	4	a
	K.G. Kashala et al., 2020 [18]	250 studies	Modified SqeezeNet model with a bypass after blocks 2, 4, 6, and 8, and Conv2D (1×1) before pooling expand blocks	– Accuracy: 81.8% – F1-score: 0.80
Classification of liver neoplasms by nosological entities	J. Zhou et al., 2021 [20]	154 studies	2.5D Faster R-CNN was used for segmentation. 3D ResNet-18 (Conv3D-based modification) was used for classification.	 Accuracy: 82.5% for distinguishing between benign/ malignant neoplasms Accuracy: 73.4% for detecting one of the six conditions (hepatocellular carcinoma, cholangiocarcinoma, metastasis, hemangioma, hyperplasia, and cyst)
	M. Rela et al., 2022 [21]	14 studies	Support vectors method, k-nearest neighbors method	 Support vectors method Accuracy: 84.6% F1-score: 0.80 k-nearest neighbors method Accuracy: 76.92% F1-score: 0.76
Segmentation of the	Y. Ding et al., 2022 [25]	30 studies	 U-Net V-Net, a modification using ResNet blocks for 3D images 	Segmentation of the kidneys: 1) Dice coefficient for the left kidney – 0.93 for U-Net – 0.92 for V-Net 2) Dice coefficient for the right kidney – 0.91 for U-Net – 0.92 for V-Net
neoplasms	Z. Lin et al., 2021 [23]	66 studies	3D U-Net	 Segmentation of the kidneys Dice coefficient: 0.97 Segmentation of kidney neoplasms Dice coefficient: 0.84 Segmentation of kidney cysts Dice coefficient: 0.54

Table 1. Continued					
1	2		3	4	5
Segmentation of the kidneys and kidney neoplasms	C.H. Hsiao 2022 [2	et al., 27]	90 studies	U-Net with ResNet-41 or EffectiveNet architectures used as encoder blocks	Segmentation of the kidneys 1) Dice coefficient (data with preprocessing and U-Net with an encoder) - 0.96 for EfficientNet-B7 - 0.95 for EfficientNet-B4, fine-tuning 2) Dice coefficient (data without preprocessing and U-Net with an encoder) - 0.95 for EfficientNet-B4, fine-tuning - 0.95 for EfficientNet-B4, fine-tuning - 0.97 for EfficientNet-B4 - 0.27 for EfficientNet-B7 - 0.27 for EfficientNet-B7
	C.H. Hsiao 2022 [2	et al., 28]	56 studies (KiTS19)	EffectiveNet-B5 (encoder); Feature pyramid network (decoder)	Segmentation of the kidneys and kidney neoplasms Dice coefficient: 0.95
Segmentation and classification of kidney neoplasms by nosological entities	M.H. Islam 2022 [2	et al.,	~1,000 scans	Six architectures - Modified VG616 - Inception v3 - ResNet50 - EANet - CCT	Classification of kidney neoplasms 1) VGG16 architecture - Accuracy: 98.2% - Mean F1-score: 0.98 - Mean AUC: 0.99 2) Inception v3 architecture - Accuracy: 61.6% - Mean F1-score: 0.59 - Mean AUC: 0.85 3) ResNet50 architecture - Accuracy: 73.8% - Mean AUC: 0.93 4) EANet architecture: - Accuracy: 77.0% - Mean F1-score: 0.77 - Mean F1-score: 0.77 - Mean AUC: 0.99 - Mean AUC: 0.97 -

Table 1. Continued				
-	2	3	4	a
	Toda N. et al., 2022 [24]	132 studies	2D U-Net for kidney segmentation 3D U-Net for neoplasm segmentation and classification	Classification of kidney neoplasms - Accuracy: 87.5% - AUC: 0.93
Segmentation and classification of kidney neoplasms by nosological entities	Zhu X.L. et al., 2022 [26]	20 studies	FS-net: source data were entered into a fine-tuned 3D U-Net. The resulting mask was pooled with the source data and entered into the fine-tuned 3D U-Net. Segmented kidney and kidney area data were received from the resulting mask. A texture analysis of the segmented data was performed to create features. A fine-tuned 3D U-Net was used for the kidney area to create features. The resulting features were used in the support vectors method.	 Segmentation of the kidneys Dice coefficient: 0.97 (KiTS19) Dice coefficient: 0.97 (own dataset) Segmentation of kidney neoplasms Dice coefficient: 0.77 (own dataset) Dice coefficient: 0.77 (own dataset)
Classification of kidney	L. Yang et al., 2022 [30]	120 studies	Features were created for manually segmented kidneys using the Pyradiomiocs library. A feedforward network was used for the features.	Classification of kidney neoplasms: AUC: - 0.76 in the pre-contrast phase - 0.77 in the nephrographic phase - 0.77 in the nephrographic phase
neoplasms and meir characteristics	M. Shehata et al., 2021 [31]	1	The following features were created for manually segmented kidneys with a neoplasm: morphological (shape assessment), textural, and functional. A feedforward network was used for the features to classify them as benign or malignant. A feedforward network was used for malignant features to distinguish between clear cell and nonclear cell cancer	Classification of benign vs. malignant kidney neoplasms – F1-score: 0.98 Classification of kidney cancer – Accuracy: 89.6%
Urinary stone detection by CT	A. Caglayan et al., 2022 [35]	I	xResNet50	Urinary stones <1 cm - Accuracy: 85% - F1-score: 0.85 Urinary stones 1–2 cm - Accuracy: 89% - F1-score: 0.89 Urinary stones >2 cm - Accuracy: 93% - F1-score: 0.93

1	2	3	4	5
	C. Daniel et al., 2022 [36]	90 studies	3D U-Net for kidney segmentation, noise reduction, and crop- ping the area of interest; 13-layer 3D CNN for classification	– AUC: 0.95 – Specificity: 0.91
/ stone detection	Y. Cui et al., 2021 [45]	117 studies	Sequential use of 3D U-Net architectures for kidney segmen- tation. The obtained data were used in five 3D U-Net architec- tures, each intended to classify one STONE score parameter.	Segmentation of the kidneys and sinuses – Dice coefficient: 0.93 Urinary stone detection – Accuracy: 90.3% – AUC: 0.96
	K. Yildirim et al., 2021 [47]	100 studies	xResNet50	- Accuracy: 97% - F1-score: 0.97