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Prospective Evaluation of the Extensibility of the Ascending Aorta Wall and its Vascular Prosthesis in a Patient with an Aneurysm with Technically Flawless Surgical Correction and Postoperative Decrease in Functional Parameters: Description of the Case

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ABSTRACT

In this clinical case, a patient who had an instrumentally detected aneurysm with the lumen expanding up to 60 mm underwent a surgically flawless prosthetic replacement of the ascending aorta. This treatment led to decreased exercise tolerance, decreased contractile function of the left ventricular myocardium at rest, and enlarged pulmonary artery. The leading factor was a decrease in the volume of systolic expansion of the aorta down to 5 mL (at the initial 13 mL), despite a noticeable increase in the extensibility and a decrease in mechanical stiffness compared with initial indexes of the affected aortic wall. In the literature review, considering mechanical extensibility and elasticity, problems in creating aortic prostheses equivalent to those for healthy biological tissues were discussed.

Keywords: aneurysm of the ascending aorta; prosthetics of the ascending aorta; extensibility; Young's modulus; systolic stretching of the aorta; coronary blood supply to the myocardium; case report.

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Проспективная оценка показателей растяжимости стенки восходящей аорты и её сосудистого протеза у пациентки с аневризмой при технически безупречной хирургической коррекции и послеоперационном снижении функциональных показателей: клинический случай

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АННОТАЦИЯ

Представлен и обсуждён клинический случай, когда у пациентки после выполнения хирургически безупречного протезирования восходящей аорты отмечалось выраженное снижение толерантности к физической нагрузке, снижение сократительной функции миокарда левого желудочка в покое и расширение лёгочной артерии вследствие усиления лёгочной артериальной гипертензии. Протезирование было выполнено в связи с инструментально выявленной при расширенном магнитно-резонансном томографическом исследовании аневризмой восходящей аорты с увеличением просвета в поперечном сечении аорты до 60 мм. Показано, что единственным и ведущим фактором к развитию негативных последствий протезирования явилось снижение объёма систолического расширения аорты до 5 мл, при исходных 13 мл, несмотря на заметное увеличение показателей растяжимости и снижения механической жёсткости по сравнению с показателями поражённой стенки аорты. Представлен обзор литературы и обсуждены в этой связи настоятельная необходимость и проблемы создания протезов аорты, эквивалентных по показателям механической растяжимости и упругости таковым для здоровых биологических тканей.

Ключевые слова: аневризма восходящей аорты; протезирование восходящей аорты; растяжимость; модуль Юнга; коронарное кровоснабжение миокарда; клинический случай.

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对一名动脉瘤患者升主动脉壁及其血管假体的伸展性 参数进行前瞻性评估,手术矫正技术完美,但术后功 能下降

Alexander V. Friedman¹, Tatiana A. Bergen¹, Dmitry A. Sirota¹, Boris N. Kozlov², Irina Yu. Zhuravleva¹, Alexandra R. Tarkova¹, Wladimir Yu. Ussov¹, Alexander M. Chernyavskiy¹

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摘要

本文介绍并讨论了一例临床病例,患者在对升主动脉进行无暇假体修复手术后,运动耐力明显下降,左心室静息时心肌收缩功能减弱,肺动脉高压加重导致肺动脉扩张。通过增强磁共振成像器械检测到升主动脉瘤,主动脉横截面的管腔扩大到 60 毫米,在这种情况下进行了假体植入术。结果表明了,尽管与病变主动脉壁的指数相比,主动脉的伸展性指数明显增加,机械硬度指数下降,但假体造成不良后果的唯一和主要因素是主动脉收缩期的扩张量从最初的 13 毫升减少到 5 毫升。本文对文献进行了综述,并就此讨论了制作在机械延伸性和弹性方面与健康生物组织相当的主动脉假体的迫切性和问题。

关键词:升主动脉瘤;升主动脉假体;伸展性;Young 模块;冠状动脉心肌血流;临床病例。

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INTRODUCTION

Surgical treatment of ascending aortic aneurysms with a >5 cm lumen expansion [1] has been the technique of choice in preventing the risk of aneurysm rupture, with a mortality rate of up to 100% in acute cases [2–4].

Several cardiac surgery techniques, involving complete or partial arch replacement, have been developed [5].

The outcomes of such replacement are assessed based on the significant decrease in the risk of mortality in such patients [2]. The quantitative assessment of physiological and biomechanical parameters of the ascending aorta, quality of life, and the presence and severity of angina and other coronary ischemia markers is often regarded as less significant [3]. This may be justified, as saving the patient's life is always the top concern.

However, a sustained decrease in the mortality rate with the surgical treatment of ascending aortic aneurysm requires further clarification of pathophysiological criteria determining the functional status of patients, possibility of recovery and vocational rehabilitation, state of the cardiac muscle, and factors affecting coronary blood supply.

The ascending aorta is a crucial anatomical and functional component of the vascular system. It provides blood supply to the cardiac muscle, which invariably occurs during diastole, within the systolic expansion volume of the ascending aorta [6]. Physiologists and sports medicine specialists [6], as well as prosthetic valve and vessel manufacturers [7], have long been interested in the elastic properties of the ascending aorta in the context of adequate blood supply to the cardiac muscle, when the aorta, which stretches during systole, collapses during diastole. However, single-center and multicenter studies of the clinical use of biophysical and biomechanical assessments of aortic elasticity are limited [4]. It has been previously demonstrated that decreased elasticity and distensibility and increased stiffness of the ascending aorta are significant pathological factors contributing to the risk of acute myocardial infarction [8, 9]. Studies of ascending aortic elasticity in cardiac surgery patients with aneurysms are equally clinically significant. Insufficient graft elasticity can be a limiting and pathological factor.

Thus, this study presents a clinical case of a female patient who failed to reach the target pO_2 level post-surgery, as well as other parameters required for a good performance status (e.g., exercise tolerance), despite uncomplicated ascending aortic replacement. These metrics did not improve, but rather worsened, and the patient has been dependent on an oxygen concentrator for breathing several months after surgery.

DESCRIPTION OF THE CASE

We present a clinical case of prospective follow-up of changes in biomechanical parameters of aortic aneurysm

during surgical treatment of a 65-year-old female (patient B-k). The patient has a history of hypertension for 10 years (with full pharmacological blood pressure control). Additionally, she has type 2 diabetes mellitus, with glucose and glycated hemoglobin levels controlled to the limit of normal with oral antidiabetic drugs. She was otherwise healthy for the last 15 years.

The patient initially presented to a neurologist with increasingly frequent episodes of dizziness and weakness with fatigue, and transient, short-term episodes of loss of speech. Critical stenosis of the internal carotid artery or its branches was suspected, and the patient was referred for ultrasound examination and carotid magnetic resonance (MR) angiography. These examinations did not confirm the carotid artery pathology. Narrowing of the internal carotid arteries or their branches by more than 15%–20% was not observed. However, carotid MR angiography showed a pathological radial expansion of the ascending aorta lumen of up to 57–60 mm. This was confirmed by MR aortography (Fig. 2*a*), and the patient was referred to the Research Institute of Cardiology of the Tomsk National Medical Research Center for consultation and cardiac surgery.

Further, the patient had preoperative coronary angiography and aortography, which confirmed the nature and extent of the aortic lesion and ruled out coronary stenosis. The proximal right coronary artery showed the most severe stenosis, of up to 35% of the lumen. Stenoses in the left coronary artery did not exceed 25% in any of its branches.

Prior to aortic replacement, the exercise tolerance threshold according to a cycle ergometer exercise test with electrocardiography (ECG) monitoring was 25 W. The test was stopped because of shortness of breath and muscular weakness. The test did not reveal ECG signs of coronary insufficiency.

As previously mentioned, the patient had magnetic resonance imaging (MRI) of the heart and aortic wall with ECG gating [8], including the thoracic aorta up to the diaphragm. In particular, heart MRI along its short and long axes was performed, which included the following:

- T1 weighted images (WI): time of repetition (TR), 500 msec; time of echo (TE), 12 msec
- T2WI: TR, 4,000 msec; TE, 25 msec
- Steady-state free precession (SSFP) images

Slice thickness: 5–8 mm; matrix: 256×392 or 256×256 . Axial T1WI chest MRI with respiration and ECG gating, with increased TR of 1,850–1,900 ms and TE of 32 ms, was performed as a component of cardiac and chest MRI with ECG gating (Fig. 1). This mode provides visualization of large thoracic vessels, including their walls. Owing to the borderline glomerular filtration rate (<30 mL/min × 1.73 m²), additional paramagnetic contrast enhancement was not used.

Following cardiac MRI, the patient underwent MRI of the ascending aorta with ECG gating, at the level of crossover with the pulmonary artery bifurcation level, in axial plane,



Fig.1. Transverse slices of T1-weighted images of the chest organs, including the thoracic aorta, at the pulmonary artery bifurcation level in patient B-k: (*a*) before prosthetic replacement of the thoracic aorta expanded due to aneurysm; critical ascending aortic aneurysm with a >6 cm lumen expansion; (*b*) after prosthetic replacement of the thoracic aorta expanded due to aneurysm; normal lumen of the ascending aorta. The descending aorta was normal before and after surgery. The pulmonary artery expanded to 27 mm after surgery, compared to 23 mm at admission. Postoperative tomography revealed an artifact in the chest area due to a wire fixator.



Fig. 2. Magnetic resonance imaging with ECG gating in patient B-k: (*a*) magnetic resonance angiography of the thoracic aorta. The lumen at the supravalvular and aortic arch levels and the distances between them, which are used to calculate the ascending aorta volume during systole and diastole and the systolic expansion volume, are shown. The turquoise horizontal line with arrows at the ends represents the tomographic slice level; (*b*) transverse tomographic slice of the ascending aorta in the wall area, with thickness measurements for the subsequent calculations of Young's modulus parameters. The measurements are marked by thin green lines, with respective values.

in the cine mode (24 cine frames per cardiac cycle), with the assessment of changes in the aortic wall thickness during a cardiac cycle (Fig. 2b) and diameter and cross-sectional area of the lumen at the study level (marked with an arrow in Fig. 2a). The cardiac MRI findings were processed using a standard method; the left ventricular end-diastolic volume, left ventricular end-systolic volume, and left ventricular ejection fraction were calculated. Moreover, biomechanical parameters of aortic distensibility were obtained based on non-contrast-enhanced cine mode MRI findings.

These measurements and a linear biophysical model [10, 11] were used to calculate the distensibility (radial expansion) of the aorta [12]:

$$Distensibility_{adj} = S_{syst} - S_{diast} / S_{diast}$$
(1)

Moreover, the distensibility adjusted for pulse pressure was calculated:

Distensibility
$$_{adj} = \frac{S_{syst} - S_{diast} / S_{diast}}{BP_{aulse}}$$
 (2),

where S_{syst} and S_{diast} are the cross-sectional areas of the aorta during systole and diastole, respectively, and BP_{pulse} is the pulse pressure (Fig. 3).

The transverse Young's modulus for the ascending aorta wall was calculated based on the findings of MR



Fig. 3. Cross-sectional dimensions and areas of the ascending aorta during systole and diastole: top row: baseline (at admission; before replacement of the aorta that expanded due to aneurysm); bottom row: after replacement with a synthetic graft; (a, c) diastole; (b, d) systole. Of note is a considerable lumen narrowing after surgery, with a relatively small distensibility of the ascending aorta.

aortography with ECG gating, according to the method well-studied in biomechanical experiments [10, 11]:

$$E = \frac{d_{diast}^{2} \times (1 - 0.25) \times BP_{pulse}}{2 \times h \times \Delta d_{pulse}} \times 133.3 \quad (3),$$

where *E* = Young's modulus (Pa),

*d*_{diast} = transverse aortic diameter during diastole,

 Δd_{pulse} = increase in the aortic diameter during systole,

0.25 = squared Poisson's ratio for the aortic wall, which is known to be 0.5 [11],

h = aortic wall thickness during diastole (Fig. 2b),

*BP*_{pulse} = pulse pressure, and

133.3 = conversion factor (mmHg to Pa).

The ascending aortic volume was calculated, from the supravalvular level to the middle of the aortic arch (between the brachiocephalic trunk and opening of the left common carotid artery), during systole and diastole. The ascending aorta was visualized as a deformed, incompressibly curved, truncated cone with the length l (length of the aortic valve-middle of the aortic arch area; Fig. 1*a*), with the base radius determined by transverse slices in the cine mode:

lower base radius, R, and upper base radius, r. In this case, the volume of the deformed truncated cone (the ascending aorta) can be with high accuracy estimated as follows [13]:

$$V = \frac{1}{3}\pi l (R^2 + Rr + r^2)$$
(4)

The systolic expansion volume of the aorta ΔV_{syst} was determined by the difference between systolic and diastolic volumes of the ascending aorta. This parameter determines the blood volume available for the coronary blood supply to the cardiac muscle during diastole, when the primary blood supply to the cardiac muscle occurs [6, 14].

The patient underwent replacement of the ascending aorta and partial arch replacement with assisted circulation, using a 35 mm synthetic graft GORE-TEX (W.L. Gore & Associates, USA). Aortic valve replacement was not performed, as no significant aortic valve insufficiency was noted, and the area of the effective hemodynamic lumen during systole was >2.0 cm². The brachiocephalic trunk ostium was implanted in the respective branch of the graft; postoperatively, no blood supply disturbances in the right common carotid artery and subclavian artery territories were observed.

No postoperative surgical complications, including inflammation, and signs of vital organ blood supply disturbances were noted. Sinus tachycardia at rest was reported (82-92 bpm), which worsened significantly on mild exertion. The preoperative glomerular filtration rate was 57-65 mL/min × 1.73 m², which was maintained after surgery. The patient required long-term oxygen support, because only with then her condition was subjectively close to normal. Imaging and clinical biochemistry studies revealed no signs of postoperative myocardial infarction. Without oxygen support using a membrane oxygen concentrator, the pO₂ level was 81%-83%; when a concentrator was used, this parameter increased to 93%-95% or higher (occasionally, at rest). Perfusion single-photon computed tomography with ^{99m}Tc-labeled beads revealed no signs of thrombosis or pulmonary embolism.

Following the surgery, the exercise tolerance decreased significantly compared to baseline and remained minimal during the inpatient postoperative period and after discharge. The patient resides on the second floor and can only get there by elevator; an outpatient MRI required the use of an oxygen concentrator.

A follow-up examination (cardiac MRI and MR elastography of the aortic wall) was performed 4 months after surgery; the findings compared to baseline are presented in Tables 1 and 2.

Aortic elasticity parameters improved dramatically following surgery; however, they still exceeded the normal value [8]. However, the systolic expansion volume of the ascending aorta (ΔV_{syst}) decreased significantly due to a decrease in the aortic diameter by 2 cm.

The postoperative Young's modulus for the aortic wall (specifically, for the ascending aortic graft) decreased, whereas the elasticity increased. However, generally, the systolic expansion volume of the aorta decreased to approximately 5 mL (Table 2), which is insufficient for adequate coronary blood supply [8]. The physical dimensions of the graft corresponded to those specified in the documents. Thus, even in the absence of significant coronary stenoses and with an ideal surgical technique of ascending aortic replacement, insufficient distensibility of the aortic wall became a critical factor, limiting exercise tolerance after surgery and contributing to left ventricular failure, although without acute myocardial infarction.

DISCUSSION

When assessing aortic stiffness, methods initially tested in animal studies are used [15, 16, 17], such as external transmission of a high-frequency mechanical wave to the aorta, using a special MRI-compatible vibration generator, followed by an MRI recording of wave transmission along the aortic wall [15, 18, 19]. This method, adapted from solid-organ elasticity studies, is commonly used [18, 19, 20].

The high-frequency method of mechanical aortic elasticity assessment allows for the calculation of this parameter throughout the anatomical study area (along the length of the aorta) [19]. However, the aortic volume at a specific level, particularly at the level of the ascending aorta, is not considered [2]. The volume of various parts of the aorta in the case of pathologies has recently become a subject of interest [15].

In this context, the distensibility of the aortic lumen during a cardiac cycle following changes in aortic pressure is a more physiological parameter [12]. Regarding the ascending aorta, it allows for direct assessment of the blood volume available for pumping into the coronary bed during diastole [12]. In the present case, this parameter allowed determining the

Table 1. Caralac magnetic resonance maging maings in patient by k before and area abilite reptacement									
	Left ventricular myocardium mass, g	LVEDV, mL	LVEF, %	LVESV, g	Left atrial volume, mL	Pulmonary artery diameter, mm			
Baseline (at admission)	165	79.4	83	165	55.7	23			
After ascending aortic replacement	161	94.2	73	161	69.4	28			

Table 1. Cardiac magnetic resonance imaging findings in patient B-k before and after aortic replacement

Note: LVEDV, left ventricular end-diastolic volume; LVEF, left ventricular ejection fraction; LVESV, left ventricular end-systolic volume. Parameters indicating the progression of heart failure (increased LVEDV, decreased LVEF, increased left atrial volume, and pulmonary artery expansion by 4 mm) are in bold text.

Table 2. Magnetic resonance elastometry of the ascending aortic wall in patient B-k before and after aortic replacement

	Young's modulus for the ascending aortic wall, Pa		ΔV _{syst} ,	
		Absolute	Adjusted = absolute/pulse pressure	mĹ
Baseline (at admission)	0,58×10 ⁶	0.0043	0.0043/25 = 1.72×10 ⁻⁴	13.28
After ascending aortic replacement	0,260×10 ⁶	0.0161	0.0161/20 = 8.05×10 ⁻⁴	4.95

exact cause of the patient's postoperative condition, which was initially attributed to undetected flaws of the surgical technique; however, the existence of these flaws was later disproved.

This demonstrates that the aorta is crucial for adequate coronary blood supply to the cardiac muscle [6, 12]. In the case of ascending aortic replacement, the graft elasticity plays a critical role [7]. It is even more relevant considering that aortic wall inflammation [24] and stiffness [25] are associated with the incidence and severity of cerebrovascular accidents. Single-center [12] and multicenter studies [8, 26] confirmed that increased aortic wall stiffness is a predictor of increased incidence of coronary disorders in patients with myocardial infarction. In patients with cardiovascular diseases that do not require cardiac surgery, drug therapy can significantly improve aortic distensibility and elasticity [27].

As previously stated, further development of ascending aortic grafts is focused on the use of synthetic and multicomponent materials with preserved elasticity, which ensure adequate diastolic blood supply to the cardiac muscle and exercise tolerance [7]. Manufacturers are aware of this issue [28, 29], which is shown in the present case: the mechanical aortic wall stiffness after surgery decreased more than twofold compared to the aorta with aneurysm before surgery, whereas the distensibility increased more than threefold (Table 2). However, considering the graft diameter, which is decreased compared to the baseline aneurysm, modern synthetic materials cannot maintain the systolic expansion volume of the ascending aorta (ΔV_{syst}).

In this regard, biological aortic grafts [29, 30] produced using special technologies from major vessels of cattle, with preserved structure of collagen and elastin fibers, provide an advantage regarding mechanical distensibility and elasticity. Currently, these are the only grafts capable of maintaining the wall distensibility of a complex hemodynamic structure such as the aorta [30]. MR elastometry can be used for aortic elasticity monitoring after replacement, with the desired frequency and duration of follow-up [8]. It can be used to assess the aortic wall and mechanical distensibility parameters in patients with ascending aortic replacement and in experimental settings.

CONCLUSION

MR elastometry provides therapeutically valuable information when used for the quantitative assessment of the biomechanical state of the ascending aorta. This should

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be considered when conducting studies in patients with aortic diseases, both atherosclerotic and due to other causes, and during prosthetic graft replacement of the ascending aorta irreversibly changed due to aneurysm.

MR elastometry with ECG gating for assessing the distensibility and calculating the Young's modulus for the damaged aortic wall currently has no alternatives, because X-ray computed tomography-based elastometry, which is methodologically equivalent, is inherently associated with radiation exposure.

MR elastometry is expected to gain more clinical use, as calculating the systolic expansion volume of the aorta is clinically relevant in other aortic biomechanics and coronary circulation disorders of various origins.

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